

Department of Physics

## Examination paper for TFY4320 Physics of Medical Imaging

**Academic contact during examination:** Pål Erik Goa

**Phone:** 959 08 026

**Examination date:** Tuesday June 6<sup>th</sup> 2017

**Examination time (from-to):** 09:00-13:00

**Permitted examination support material:** Code C

- Karl Rottmann: Matematisk Formelsamling.
- Barnett and Cronin: Mathematical Formulae.
- Øgrim og Lian: Størrelser og enheter i fysikk og teknikk.
- A specified, simple calculator is permitted.

**Other information:** Each sub-question (1a, 1b, etc) carries equal weight in the evaluation. Exam might be answered in English or Norwegian.

**Language:** English

**Number of pages (front page excluded):** 5

**Number of pages enclosed:** 0

Informasjon om trykking av eksamensoppgave

Originalen er:

1-sidig  2-sidig

sort/hvit  farger

skal ha flervalgskjema

Checked by:

\_\_\_\_\_  
Date

\_\_\_\_\_  
Signature

## Some useful expressions and values.

$$\begin{aligned}
 I &= NE \\
 I &= I_0 e^{-\int \mu(x) dx} \\
 S &= \varepsilon A (I_P + I_S) \\
 C &= \frac{I_1 - I_2}{I_1} \\
 k &= \frac{S_1 - S_2}{STD_s} \\
 D &= EN_0 \left( \frac{\mu_{en}}{\rho} \right) \\
 \varepsilon &= \frac{N_{out}}{N_{in}} \\
 p(s, \theta) &= -\ln \frac{I}{I_0} = \int_A^B \mu(s, t) dt \\
 HU &= 1000 \cdot \frac{\mu - \mu_w}{\mu_w} \\
 R_c &= \frac{d(L+z)}{L} \\
 g &= \frac{d^2}{4\pi L^2} \frac{d^2}{(d+t)^2} \\
 t &= \frac{6d}{\mu L - 3} \\
 S &= S_0 (1 - e^{-TR/T_1}) e^{-TE/T_2} \\
 S &= \frac{S_0 (1 - e^{-TR/T_1}) \sin \theta e^{-TE/T_2}}{1 - \cos \theta e^{-TR/T_1}} \\
 f\lambda &= c \\
 c &= c_0 + v\beta \\
 \beta &= 1 + B/2A \\
 f_d &= \frac{\pm 2f_0 v \cos \theta}{c}
 \end{aligned}$$

Table 1: Linear attenuation coefficients [1/cm]

keV	Water	Soft Tissue	Bone	Calc.	Se
20	0.81	0.87	7.68	9.29	216
511	0.097				

## Problem 1: X-ray mammography

### 1 a

Start from the definition of the visibility  $k$  and derive the expression of  $k$  given below for a small object of dimension  $x$  with linear attenuation coefficient  $\mu_2$  inside a large object of thickness  $t$  and  $\mu_1$ . State any assumptions or simplifications you do as part of this derivation as well as the definition of the additional parameters required.

$$k = (1 - e^{-\Delta\mu x}) \sqrt{\frac{\varepsilon A N_0 e^{-\mu_1 t}}{1 + R}} \quad (1)$$

### 1b

Calculate the resulting surface dose to the patient in units of mGy, given the following values:

- Breast tissue thickness: 2 cm.
- Dimension of calcification: 0.1 mm.
- Scattering ratio: 0.5.
- Detector: Amorphous Se, 0.1 mm thickness.
- Visibility  $k = 5$ .
- X-ray effective energy 20 keV.

The soft tissue mass energy absorption coefficient at 20 keV is  $0.56 \text{ cm}^2/\text{g}$ .

### 1c

Describe how a suitable X-ray spectrum can be generated for the above situation, including choice of anode material, acceleration voltage and possible filters. Draw the approximate shape of the resulting spectrum.

## Problem 2: Nuclear Medicine Imaging

### 2a

The following simplified expression/model for the number of counts in a gamma camera was discussed in the course:

$$\#counts \propto \int_0^{t_s} A_0 e^{-\lambda t} dt \cdot Y_\gamma (1 - \bar{\phi}_\gamma) \cdot g \cdot \varepsilon_D(E_\gamma) \quad (2)$$

- Use a figure to illustrate the process described by this model, and define/explain each of the terms.
- Based on the model, discuss problems/challenges in order to reconstruct quantitative SPECT images (images with activity instead of counts).
- Identify one additional effect that needs to be corrected for in quantitative SPECT imaging (not included in the model).

### 2b

Given a PET-ring with diameter 80 cm and filled with one ring of detectors consisting of 9x9 LSO crystals, each with dimensions 4x4x25 mm.

- Calculate the geometric efficiency of the PET-ring.
- Calculate the maximum spatial resolution.
- Estimate the coincidence detection probability for a point source. State any assumptions made as part of your estimate.
- Estimate the coincidence detection probability for a point source positioned in the center of a water-filled cylinder with diameter of 20 cm.

The non-colinearity effect is 2.2 mrad and the linear attenuation coefficient of LSO at 511 keV is 0.88 1/cm.

## Problem 3: Magnetic Resonance Imaging

### 3a

Explain the two physical interaction processes expressed by the following equations:

$$\vec{N} = \vec{\mu} \times \vec{B} \quad (3)$$

$$\frac{d\vec{J}}{dt} = \vec{N} \quad (4)$$

Use the above to derive the equation of motion for the magnetic moment in an external field, and define the gyromagnetic ratio  $\gamma$ .

### 3b

Given a 2D spin-echo MR-sequence with the following parameters: TE = 20 ms, TR = 1200 ms, field-of-view = 256x256 mm, image matrix 128x128, slice thickness = 5 mm, number of slices = 10, rf-pulse bandwidth: 2 kHz. Answer the following questions, and justify your answers:

- What is the total duration of the MR-scan?
- What is the spatial resolution?
- What is the amplitude of the slice-select gradient (in units of mT/m)?
- Estimate the maximum number of slices that can be included without increase in scan-time.

The gyromagnetic ratio for protons is 42.58 MHz/T.

### 3c

Draw up the complete sequence diagram for the above MR-sequence. Include one line for each of the following parameters:

- rf-pulses.
- Slice-select gradient.
- Frequency-encoding gradient.
- Phase-encoding gradient.
- Transverse magnetization, including the position of the spin-echo.
- Signal acquisition.

## Problem 4: Ultrasound Imaging

### 4a

- Describe the two main effects that governs the choice of frequency in normal pulse-echo imaging.
- Describe the main contrast mechanisms in pulse-echo imaging.

### 4b

In figure ?? below you see an ultrasound image before and after the signal-processing applied as part of matlab-exercise 7 in the course.

- Describe and explain the origin of the noise as seen in the left image.
- Describe the physical mechanism of how it is possible to reduce this noise.
- Describe the post-processing procedure used in order to achieve this effect.

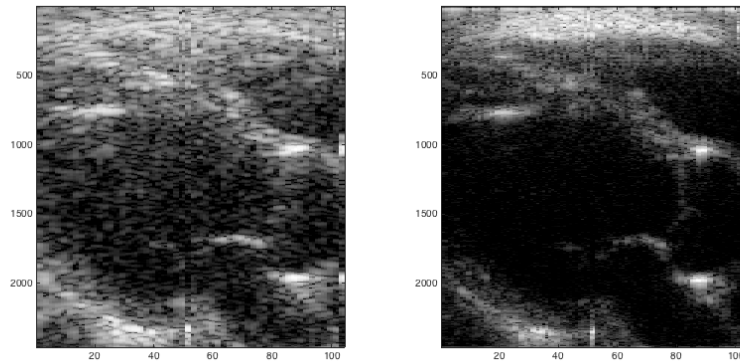


Figure 1: Ultrasound Image before (left) and after (right) signal processing.